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Fast energy modulation within the beamline momentum acceptance: a clinical feasibility study

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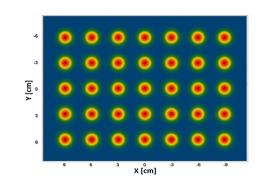
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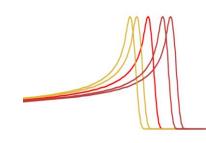
INTRODUCTION	MATERIALS AND METHODS
Pencil beam scanning proton therapy is delivered as a sequence of iso-energy dose layers, changing progressively while scanning across the target. [1]	Beam properties For a relevant set of particles off-momentum between 150 and 230 MeV, we analysed clinically significant parameters:
Changing energy requires changing magnetic fields in several slow-settling beamline magnets. We investigated into modulating proton energy within the beamline momentum acceptance with an upstream degrader to minimise dead time during beam delivery.	 Beam position, & Shape, Range, Transmission. Clinical case Indication: cranial glioma Prescribed dose: 1.8 GyRBE CTV volume: 183.9 cm³ PTV volume: 279.6 cm³ Plan optimization: SFUD Energy layers: 48

RESULTS

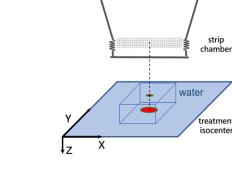
Beam properties characterisation



Spot position median error < 1mm</p>



Dept-dose profile γ (1%/1mm) > 90% **Range** median error 1.16 mm



Spot shape
median error < 1mm</p>



Transmission 14% median decrease compared to clinical settings

Clinal plan verification at target depth

Treatment has been verified in a similar manner as our clinical plans [2] using a cross-calibrated array of ionisation chambers (PTW Octavius 1500XDR, Freiburg, D) aligned at isocenter.

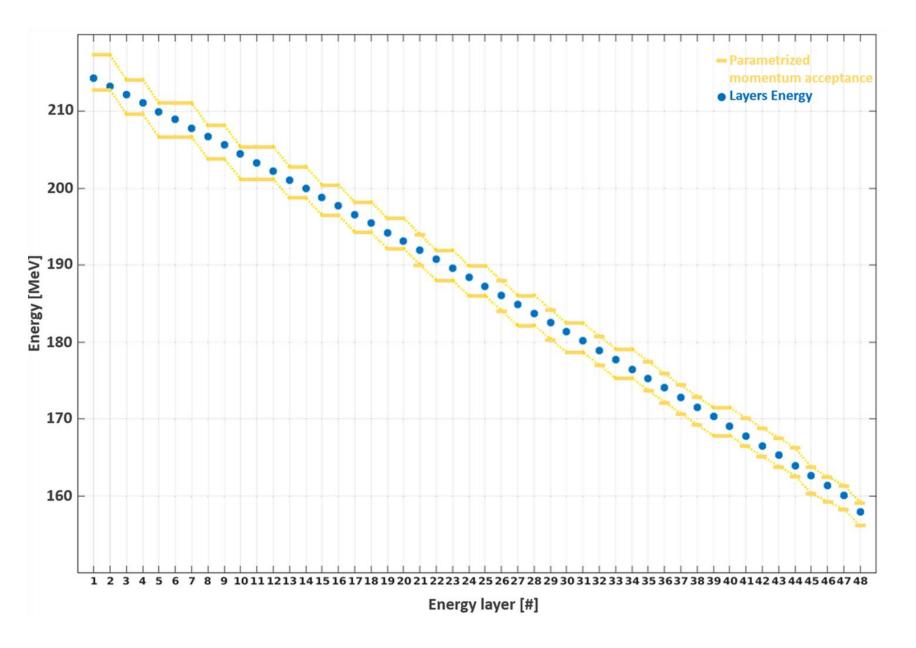
The plan has been delivered twice, using the standard settings for clinical treatments or making use of the beamline acceptance to reduce the number of full beamline tuning.

Clinical plan energy modulation within the beamline momentum acceptance

The plan's 48 energy layers are represented (from high to low energy) as **blue dots**.

The yellow lines represent the beamline momentum acceptance calculated around specific proton energies to ensure continuous coverage of the beam ranges used in the plan.

Overall, 16 beamline re-tunes could be avoided by associating consecutive energy layers to acceptance bands. Delivery time was reduced by 12%, on a machine with nominal energy switching time about 100 ms.



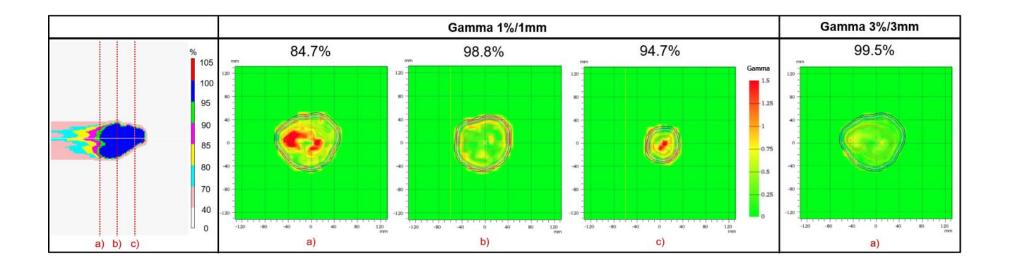
Clinal plan analysis

The two deliveries have been compared using Gamma (1%,1mm) - standard settings considered as reference. Gamma maps and pass rates are reported for three verified planes located respectively at 19.6 cm (a), 23.7 cm (b) and 28.2 cm (c) water equivalent depths.

Largest discrepancies with respect to clinical settings were measured for a proximal layer (a) located in a region of steep dose gradients. The distortions were however below the (3%,3mm) Gamma criteria that is commonly used in the clinic (rightmost panel).

The measurement was performed at three depths located proximally, roughly in the middle and distally in the field using a stack of Polymethyl Methacrylate (PMMA) slabs.





CONCLUSIONS	REFERENCES AND FUNDING
The potential of energy regulation within momentum acceptance has been investigated on a gantry based medical beamline. Provided that range errors and transmission losses introduced by the distortion of the beam spectra are compensated for, fast energy changes could be achieved under experimental settings with negligible distortions in the delivered dose distribution and without ad-hoc beamline modifications.	 [1] E. Pedroni, R. Bearpark, T. Böhringer, A. Coray, J. Duppich, S. Forss, D. George, M. Grossmann, G. Goitein, C. Hilbes, M. Jermann, S. Lin, A. Lomax, M. Negrazus, M. Schippers, G. Kotrle, The PSI Gantry 2: A second generation proton scanning gantry, Z. Med. Phys. (2004). <u>https://doi.org/10.1078/0939-3889-00194</u>. [2] S. Safai, C. Bula, D. Meer, E. Pedroni, Improving the precision and performance of proton pencil beam scanning, Transl. Cancer Res. (2012). <u>https://doi.org/10.3978/j.issn.2218-676X.2012.10.08</u>. This project was supported by the Swiss National Science Foundation (SNF) with the grant 185082 New concept for adaptive real time tumour tracking.